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Neural representations of concurrent sounds with overlapping spectra in rat inferior colliculus: Comparisons between temporal-fine structure and envelope

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ABSTRACT

Perceptual segregation of multiple sounds, which overlap in both time and spectra, into individual auditory streams is critical for hearing in natural environments. Some cues such as interaural time disparities (ITDs) play an important role in the segregation, especially when sounds are separated in space. In this study, we investigated the neural representation of two uncorrelated narrowband noises that shared the identical spectrum in the rat inferior colliculus (IC) using frequency-following-response (FFR) recordings, when the ITD for each noise stimulus was manipulated. The results of this study showed that recorded FFRs exhibited two distinctive components: the fast-varying temporal fine structure (TFS) component (FFR_{TFS}) and the slow-varying envelope component (FFR_{ENV}). When a single narrowband noises were presented alone, the FFR_{TFS}, but not the FFR_{ENV}, was sensitive to ITDs. When two narrowband noises were presented simultaneously, the FFR_{TFS} took advantage of the ITD disparity that was associated with perceived spatial separation between the two concurrent sounds, and displayed a better linear synchronization to the sound with an ipsilateral-leading ITD. However, no effects of ITDs were found on the FFR_{ENV}. These results suggest that the FFR_{TFS} and FFR_{ENV} represent two distinct types of signal processing in the auditory brainstem and contribute differentially to sound segregation based on spatial cues: the FFR_{TFS} is more critical to spatial release from masking.

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1. Introduction

In natural environments, both humans and animals often listen to multiple-source sounds with both temporal and spectral overlaps. The ability to perceptually segregate mixed acoustic waves into different auditory streams, a process known as "auditory scene analysis" (Bregman, 1990), is crucial for survival. Several cues are employed by the auditory system to achieve this streaming, including fundamental frequency (F_0), onset time, and a few spatial cues such as interaural time difference (ITD) (Moore and Gockel, 2002).

The improvement of signal detection/perception when

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(perceived) spatial separation exists between multiple sound sources has been a long-studied psychophysical phenomenon, often referred to as "spatial release from masking" (SRM) (Hirsh, 1950). Previous behavioral studies have provided evidences demonstrating the beneficial effects of (perceived) spatial separation for both humans (Bronkhorst and Plomp, 1988; Freyman et al., 2001; Kidd et al., 1998; Li et al., 2004; Shinn-Cunningham et al., 2001) and animals (e.g., Bee, 2008; Du et al., 2009, 2012; Hine et al., 1994; Schmidt and Römer, 2011). Listeners with impaired hearing usually show reduced effects of SRM (Best et al., 2011; Ching et al., 2011; Peissig and Kollmeier, 1997). Therefore, it is of great interest to understand the underlying neural mechanisms.

To date, most electrophysiological studies in this line of research have focused on some non-spatial segregation cues such as F_0 (Fishman et al., 2014; Keilson et al., 1997), difference frequency (i.e. beats) (Bodnar and Bass, 1999, 2001a, 2001b), sound level







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(Nakamoto et al., 2010; Sinex and Li, 2007), and onset synchrony (Bidet-Caulet et al., 2007). Notably, the acoustic stimuli used in these studies had distinctive spectral features that tagged their sources readily, including pure tones with different frequencies (Bidet-Caulet et al., 2007), different harmonic tones (Fishman et al., 2014; Sinex and Li, 2007), vowels with different periodic components (Keilson et al., 1997; Sayles et al., 2016), and narrowband noises (NBNs) with different frequency ranges (Witten et al., 2010). It remains an open question how mixed sounds with overlapping spectra are resolved by auditory neurons (Day et al., 2012; Keller and Takahashi, 2005), which is often the case in natural environments.

When complex sounds reach the ear, the peripheral auditory system filters the sound waves into narrowband channels through a series of band-pass filters. For each of the narrowband channels, the output signals are further decomposed into the fast fluctuating temporal fine structures (TFSs) and the slowly varying envelopes (Moore, 2008). The contributions of TFS and envelope in auditory processing have long been debated. One notion suggests that while the envelope alone is sufficient for hearing content of speech sounds in quiet, the TFS information plays a crucial role in speech recognition under noisy situations (e.g., Apoux et al., 2013; Lorenzi et al., 2006; Smith et al., 2002; Zeng et al., 2004). However, how the TFS and envelope components contribute to the segregation of concurrent sounds is still poorly understood, especially when interaural integration is involved (Swaminathan et al., 2016).

Frequency following responses (FFRs) are sustained electrical potentials of neuron populations that synchronize to periodicities of low- and middle-frequency sounds (Chandrasekaran and Kraus, 2010; Du et al., 2011; Marsh and Worden, 1969; Moushegian et al., 1973; Weinberger et al., 1970; Worden and Marsh, 1968). Human scalp-recorded FFRs show a response limit up to 1.5 kHz (Glaser et al., 1976), and intracranially recorded FFRs in rats show a response limit up to 4 kHz (Ping et al., 2008). In humans, scalprecorded FFRs can be evoked by a variety of sounds, from simple tones (Chimento and Schreiner, 1990; Galbraith, 1994) to complex sounds such as speech syllables (Aiken and Picton, 2008; Akhoun et al., 2008; Krishnan, 2002; Russo et al., 2004; Song et al., 2008; Wong et al., 2007) and music (Musacchia et al., 2007). FFRs have been shown to be behaviorally and cognitively relevant, and subject to attentional modulation (Du et al., 2012; Galbraith et al., 1998; Hairston et al., 2013; Hoormann et al., 2004; Lehmann and Schönwiesner, 2014), short-term training (Skoe et al., 2013; Song et al., 2008), and long-term experience (Chandrasekaran and Kraus, 2010; Musacchia et al., 2007; Wong et al., 2007). Release from masking based on binaural spatial cues for FFR has been reported (Du et al., 2009, 2012; Wilson and Krishnan, 2005). Interestingly, both human (Lehmann and Schönwiesner, 2014) and animal studies (Du et al., 2011) have confirmed that FFRs precisely represent concurrent periodical-stimulus sources, with components of different frequency being clearly separated in the FFR spectra. Also, previous reports have shown that FFRs can represent the spectral information conveyed in both the TFS and the envelope components of narrowband noises (Wang and Li, 2015) and speech sounds (Aiken and Picton, 2008; Ananthakrishnan et al., 2016; Skoe and Kraus, 2010). Therefore, FFRs are useful for investigating not only stream segregation that occurs at the brainstem level but also specific representations of the TFS and envelope components (Du et al., 2011).

Intracranial-recorded FFRs have been reported recently in inferior colliculus (IC) of anesthetized rats (Du et al., 2009; Ping et al., 2008; Wang and Li, 2015) and amygdala of awake rats (Du et al., 2012). Particularly, the IC, which is the brainstem hub for auditory processing from lower nuclei converge (Schreiner and Winer, 2005), is generally considered as the major source of

scalp-recorded FFRs (Chandrasekaran and Kraus, 2010; Smith et al., 1975; Sohmer et al., 1977).

To examine the brainstem representation of concurrent sounds with overlapping spectra and the effect of ITD on source segregation of the concurrent sounds, in this study we used pairs of uncorrelated NBNs with the identical center frequency and bandwidth to evoke FFRs in rat IC when the ITD of each NBN was manipulated separately. The TFS and envelope components of FFRs were extracted and investigated separately, focusing on their sensitivities to the ITD.

2. Materials and methods

2.1. Animal preparation

Sixteen young-adult male Sprague-Dawley rats (270–359 g, purchased from the Vital River Experimental Animal Company, Beijing) were used in this study. They were anesthetized with 10% chloral hydrate (400 mg/kg i.p.). The state of anesthesia was monitored throughout the experiment and maintained by supplemental injection of the same anesthetic. Stainless steel electrodes (10–20 k Ω) insulated by silicon tubes (0.3 mm in diameter) except at the 0.25-mm-diameter tip (Du et al., 2009, 2012; Wang and Li, 2015) were inserted in the left or right central nucleus of the IC (left: n = 8; right: n = 8). Based on the stereotaxic coordinates of Paxinos and Watson (1997), the coordinates of the aimed IC site referenced to Bregma were: AP, -8.8 mm; ML, ±1.5 mm; DV, -4.5 to -5.0 mm.

The treatments of animals in this study were in accordance with the Guidelines of the Beijing Laboratory Animal Center. All experimental procedures were approved by the Committee for Protecting Human and Animal Subjects in the School of Psychology and Cognitive Sciences at Peking University.

2.2. Apparatus and stimuli

Acoustic stimuli were processed through a Tucker-Davis Technology RZ6 auditory processor and presented by two MF1 loudspeakers. For the close-field sound delivery, two 10-cm PVC tubes were connected to the tips of the loudspeakers, with the other ends being inserted into each of the rat's ear canals. All stimuli were calibrated using a Larson Davis Audiometer Calibration and Electroacoustic Testing System (AUDit and System 824), and the sound pressure level (SPL) was 70 dB for each loudspeaker.

For each rat, a pair of uncorrelated NBNs (24414-Hz sampling rate, 16-bit amplitude quantization) with a center frequency of 1200 Hz and a bandwidth of 400 Hz were drawn from a pool of 500 NBN pairs, which were generated by passing Gaussian white noises through a 512-point filter with MATLAB (MathWorks, Natick, MA) (see Fig. 1A for an example). Since16 rats were used in this study, a total of 16 different pairs of NBNs were used. These NBN pairs were chosen for their low mutual coherences (mean = 0.070 ± 0.016 SD). To avoid the spectral dominance from one single sound of a NBN pair, the coherence between each individual sounds and the summation of the NBN pair was checked to make sure that the coherence difference within each pair was minimum (mean coherence difference = 0.067 ± 0.056 SD). The stimulus duration was 150 ms with 5-ms Hanning onset/offset ramps. The (offset-onset) interstimulus interval was 250 ms.

Under the single-source condition, only one sound from the NBN pair was presented binaurally with the interaural time difference (ITD) of either +0.16 ms (ipsilateral-leading, referenced to the recording site) or -0.16 ms (contralateral-leading, referenced to the recording site). The ITDs of ± 0.16 ms were chosen because this is not only the natural ITD limit of low-frequency fine structures for

adult rats as measured by Koka et al. (2008), but also below onequarter of the period of the center frequency (0.21 ms) allowed by the 24414-Hz-sampling-rate recording system.

Normally, when the ITD is +0.16 ms, the stimulus image would be perceived as from the ipsilateral ear; when ITD is -0.16 ms, the stimulus image would be perceived as from the contralateral ear (Fig. 1B). Under the double-source condition, each of the two sounds in a NBN pair was presented binaurally, with an ITD of either +0.16 ms or -0.16 ms, leading to 4 laterality configurations between the two NBNs. For the sake of clarification, the NBNs used in both single- and double-source conditions were named as "source A", while the NBNs only used in double-source conditions were named as "source B". Therefore, when source A and source B share the same ITD, they are perceived as from the same location ("perceived co-location"); when the ITD of source A is different from the ITD of source B, they are perceived as from different locations, with one at the ipsilateral ear and the other at the contralateral ear ("perceived spatial separation") (Fig. 1B).

Acoustically evoked potentials were recorded in a soundattenuating chamber, amplified by a TDT RA16P Medusa preamplifier, and filtered through a 5- to 10,000-Hz online band-pass filter (with a 50-Hz notch). For each condition, stimuli were presented either in the original polarity or in the inverted polarity, and the neural responses associated with each of the stimulation polarities were averaged 100 times. All the stimulation conditions were presented in random order for each rat. Online recordings were processed with TDT Biosig software, digitized at 24414 Hz, and stored in a disk for off-line analyses.

2.3. Data analyses

Inverting the polarity of NBN waves reversed the stimulus fine structures, while leaving the envelope unchanged. Therefore, the envelope component of FFRs (FFR_{ENV}) could be extracted by averaging the summation of FFRs to stimulus with opposite polarities, and the fine structure components of FFRs (FFR_{TFS}) could be extracted by subtracting response to the inverted stimulus from that to the original stimulus and dividing the results of subtraction by two (Aiken and Picton, 2008; Joris, 2003; Skoe and Kraus, 2010).

The response latency under each condition was determined by the onset peak using Matlab function *findpeaks* and further confirmed manually. The onset peak was defined as the first positive peak in FFR_{ENV} that was two standard deviations above the mean amplitude of the 150-ms baseline activity recorded in quiet before the stimulus onset in each stimulation condition. For every FFR_{ENV} and FFR_{TFS} component, a 150-ms fragment starting from the response onset was used for the following analyses.

To examine the synchronization between FFRs and NBN stimuli, the stimulus-response coherence (S-R coherence) was calculated. The coherence between two signals *x* and *y* (C_{xy}) is a function of frequency (*f*), and defined as $C_{xy} = |P_{xy}(f)|^2 / P_{xx}(f)P_{yy}(f)$, where $P_{xy}(f)$ represents the cross spectral density of *x* and *y*, and $P_{xx}(f)$ and $P_{yy}(f)$ represent the power spectral densities of *x* and *y*, respectively (Middleton et al., 2006; Weiss and Mueller, 2003, 2005). The TFS and envelope components of the NBN stimuli were extracted separately using Hilbert transform (Smith et al., 2002), the S-R coherence for the TFS component was calculated between FFR_{TFS} and the stimulus TFS, and the S-R coherence for the envelope component was calculated between the FFR_{ENV} and the stimulus envelope.

In this study, the frequency resolution of the coherence analysis was 6.7 Hz, and a moving Hanning window with a length of 512 data points and 75% overlap was chosen. The resulting coherence values range from 0 to 1, and measure the linear similarity between the FFRs and the stimuli. More specifically, a coherence of 1 represents perfect linear synchronization, which requires constant phase shift and amplitude ratio between the two signals at a particular frequency. Meanwhile, a coherence of 0 indicates



Fig. 1. Schematic of the stimulus and conditions. A: An example of narrowband noise used in this study, which is decomposed into TFS component and envelop component with Hilbert transform. The FFT spectrums of each component were also shown. B: A diagram of the stimulus conditions. The perceived locations of each sounds was marked by dashed circles.

complete lack of linear synchronization (Levy et al., 2000; Middleton et al., 2006; Rosenberg et al., 1989). For comparisons across different conditions, the S-R coherence value for each FFR_{TFS} and that for each FFR_{ENV} were averaged across the frequency respectively. Based on the spectrum of the NBN stimuli, the frequency range of averaging was 1000–1400 Hz for the TFS component, and 0 to 400 Hz for the envelope component.

Moreover, to compare the synchronization to each NBN sound in the double-source conditions, Δ Coh was calculated as the normalized difference between the S-R coherence with source A and source B: Δ Coh = $\frac{|coherenceA-coherenceB|}{coherenceA+coherenceB}$. Therefore, Δ Coh could be interpreted as the ability to convey information of individual sound by FFRs. A higher Δ Coh suggests more exclusive representation of either source A or B, and a Δ Coh of 0 suggests equal contribution of the two sources.

2.4. Statistical analyses

Statistical analyses were performed with IBM SPSS Statistics 20 software (Chicago, IL, USA). To evaluate the effects of different

stimulus conditions on S-R coherence, within-subjects repeated measures analyses of variance (ANOVAs), paired *t*-tests, Student's *t*-tests, and Pearson correlation tests were conducted. The coherence values were Fisher-*z* transformed before being submitted to statistical tests, while the results presented in figures were based on the original coherence values. Since no significant differences were found between the two IC recording sites (left IC, right IC), data from both sides of the IC were pooled together for all the analyses. All *p*-values of multiple comparisons were adjusted using Bonferroni correction.

2.5. Histology

After all recording sessions were completed, rats were sacrificed with an overdose of chloral hydrate. The recording sites were marked with a DC current (500 μ A for 10 s) via the inserted electrodes. The brains were removed and stored in 10% formalin with 30% sucrose and sectioned at 55 μ m in the frontal plane in a cryostat (-20 °C). Sections were examined to determine locations of recording electrodes.



Fig. 2. Histology results and FFR examples. **A:** Histological examination of recording sites in 16 rats showed that 16 of 16 electrodes were precisely located in the central nucleus of IC (CIC), with 8 electrodes inserted in the left CIC and 8 electrodes inserted in the right CIC. DCIC, dorsal cortex of IC; ECIC, external cortex of IC. **B:** An example of the extracted FFR_{TFS} (*left column*) and FFR_{ENV} (*right column*). Both the waveforms (*upper row*) and the FFT spectrums (*lower row*) were shown.



Fig. 3. An example of S-R coherence as functions of frequency for FFR_{TFS} (*left*) and FFR_{ENV} (*right*) from a recording site under single-source condition with a contralateral-leading sound named as source A. The S-R coherence with source A was plotted in red, and the S-R coherence with an uncorrelated source B was plotted in blue.

3. Results

According to the histological examination, all the 16 electrodes were located precisely in the center nucleus of IC (Fig. 2A), and descriptions and statistical analyses were based on the data from all the recording sites.

3.1. The reliability of representations of noise stimuli by FFR_{TFS} and FFR_{ENV}

NBN stimulus evoked robust IC FFRs under each of the stimulation conditions, and the extracted FFR_{TFS} and FFR_{ENV} showed similar spectra with the noise-stimulus TFS (around the center frequency of 1200 Hz) and the noise-stimulus envelope (between 0 and 400 Hz), respectively (see Fig. 2B for examples).

Under the single-source conditions, only one NBN sound (i.e. source A) was presented. The averaged stimulus-response coherence (S-R coherence) between FFR and the corresponding source A was 0.455 ± 0.060 SD for the TFS component, and 0.316 ± 0.108 SD for the envelope component. To further confirm that the S-R coherence analysis could reveal the stimulus specific information conveyed by FFRs, the S-R coherence values between FFR and source A were compared with the S-R coherence values between



Fig. 4. Comparisons of S-R coherence values across different single-source conditions for FFR_{TFS} and FFR_{ENV}. Error bars: SE; **p < 0.01.

the same FFR segment and the unpresented, uncorrelated source B. Fig. 3 shows an example from one recording site under the condition with an ipsilateral-leading stimulus. The S-R coherence of TFS and that of envelope were plotted as functions of frequency. The results showed that while the S-R coherence with source B remained low across all frequencies, the S-R coherence with source A exhibited increased power in the TFS spectra range for FFR_{TFS} and envelope spectra range for FFR_{ENV}. Paired-*t* tests further confirmed this observation, showing that for both TFS and envelope, S-R coherence with source A in the corresponding spectra range was significantly higher than the S-R coherence with source B (for all recording sites and both single-source conditions, *p* < 0.001).

3.2. ITD sensitivity of FFR_{TFS} and FFR_{ENV} under the single-source conditions

For comparisons between different single-source conditions, FFR_{TFS} and FFR_{ENV} exhibited different sensitivity to the ITD (Fig. 4). For FFR_{TFS}, a paired-*t* test showed significant higher S-R coherence with the ipsilateral-leading stimulus (mean = 0.448 ± 0.060 SD) than that with the contralateral-leading stimulus (mean = 0.399 ± 0.058 SD) ($t_{15} = 3.726$, p = 0.002).

However, for FFR_{ENV}, no significant difference occurred between the S-R coherence with the ipsilateral-leading stimulus (mean = 0.301 ± 0.096 SD) and that with the contralateral-leading stimulus (mean = 0.306 ± 0.101 SD) ($t_{15} = 0.902$, p = 0.381). Therefore, the linear synchronization between the FFR_{TFS} and the stimulus TFS was affected by the stimulus ITD with a preference towards the ipsilateral-leading sounds, and the linear synchronization between the FFR_{ENV} and the stimulus envelope appeared to be independent of the stimulus ITD.

Pearson correlation test was conducted between the S-R coherence of FFR_{TFS} and the S-R coherence of FFR_{ENV}, and no significant correlation between these two components was found (r = -0.229, p = 0.208, n = 32).

3.3. Effects of concurrent sounds

As a concurrent sound was introduced, both the averaged source-A S-R coherence values of FFR_{TFS} and those of FFR_{ENV} decreased compared with single source conditions (paired *t*-tests, all p < 0.001), indicating a degradation in the accuracy of target (source-A) synchronization.

For the double-source FFR_{TFS}, a 2×2 (source-A ITD: ipsilateral leading, contralateral leading; associated laterality configuration: perceived spatial separation, perceived co-location) repeated-



Fig. 5. Comparisons of source-A S-R coherence values (*upper row*) and source-B S-R coherence values (*lower row*) across double-source conditions for FFR_{TFS} (*left column*) and FFR_{ENV} (*right column*). Error bars: SE; **p < 0.01.

measures ANOVA demonstrated a significant main effect of the source-A ITD ($F_{1, 15} = 89.190$, p < 0.001) and the laterality configuration ($F_{1, 15} = 9.485$, p = 0.008), and, most importantly, significant interaction ($F_{1, 15} = 68.801$, p < 0.001) on the S-R coherence with source A. Additional paired *t*-tests showed that the S-R coherence with an ipsilateral leading source A was significantly higher under



Fig. 6. Comparisons of the normalized differences between the source-A S-R coherence and the source-B S-R coherence (Δ Coh) in the perceived-spatial-separation conditions and the perceived-co-location conditions. Error bars: SE; **p < 0.01.

the perceived-spatial-separation conditions (mean = 0.319 ± 0.049 SD) compared to that under the perceived-co-location conditions (mean = 0.231 ± 0.033 SD) ($t_{15} = 6.702$, p < 0.001). Opposite effect of laterality configuration was found for the S-R coherence with a contralateral-leading source A, which was significantly decreased when ITD disparity was introduced between source A and source B (mean = 0.161 ± 0.037 SD) compared with that under the perceived-co-location conditions (mean = 0.207 ± 0.032 SD) ($t_{15} = 9.014$, p < 0.001) (Fig. 5).

Since source A and source B were interchangeable between the two NBNs, the same analyses were also conducted for the S-R coherence with source B. As expected, similar patterns of changes across conditions were observed. A repeated-measures ANOVA also found significant main effects of source-A ITD and laterality configuration and their interaction (main effect of source-A ITD: $F_{1, 15} = 40.589$, p < 0.001; main effect of laterality configuration: $F_{1, 15} = 5.143$, p = 0.039; interaction effect: $F_{1, 15} = 33.097$, p < 0.001). The S-R coherence with the ipsilateral-leading source B also benefited from ITD disparity and showed markedly larger values when source A was contralateral-leading, and the S-R with the contralateral-leading source B was decreased by the presence of a ipsilateral-leading source A (paired *t*-tests, both p < 0.001) (Fig. 5).

The source-A S-R coherence and the source-B S-R coherence of the FFR_{TFS} under different double-source conditions were further examined. Under the perceived spatial separation condition, the S-R coherence with the ipsilateral-leading sounds were stronger than those with the contralateral-leading sounds, whether the ipsilateral-leading sounds were source A ($t_{15} = 5.781$, p < 0.001) or source B ($t_{15} = 9.648$, p < 0.001). Meanwhile, under the perceived co-location condition, no significant differences were found

between the S-R coherence with source A and those with source B (ipsilateral co-location condition: $t_{15} = 0.241$, p = 0.813; contralateral co-location condition: $t_{15} = 1.051$, p = 0.310). Δ Coh were further introduced by calculating the normalized difference between the source-A S-R coherence and the source-B S-R coherence (for details see Materials and methods). A two-tailed Student's ttest showed that the Δ Coh under the perceived spatial separation condition (mean = 0.307 + 0.157 SD) was significantly larger than that under the perceived co-location condition $(\text{mean} = 0.094 \pm 0.064 \text{ SD}) (t_{62} = 6.886, p < 0.001)$, indicating that the extraction of individual sounds benefited from perceived spatial separation between source A and source B based on ITD disparity, and the TFS information of the preferred source could be represented with a relatively better "signal-to-noise ratio" in IC (Fig. 6).

However, for FFR_{ENV}, two-way repeated-measures ANOVAs did not show significant main effects of source-A ITD ($F_{1, 15} = 1.133$, p = 0.304) and laterality configuration ($F_{1, 15} = 3.884$, p = 0.067) on the S-R coherence with envelope of source A. The interaction was not significant ($F_{1, 15} = 2.370$, p = 0.145). The same results was also demonstrated for source-B S-R coherence (main effect of ITD: $F_{1, 15} = 2.543$, p = 0.132; main effect of laterality configuration: $F_{1, 15} = 0.643$, p = 0.435; interaction effect: $F_{1, 15} = 0.960$, p = 0.343) (Fig. 5). The S-R coherence with source A and that with source B showed no difference across all four double-source conditions (paired-*t* tests, all p > 0.05). Also, no difference in Δ Coh was found between the perceived-spatial-separation condition and the perceived-co-location condition ($t_{62} = 1.350$, p = 0.182) (Fig. 6). In summary, unlike the FFR_{TFS}, the FFR_{ENV} was not sensitive to the ITD cue.

4. Discussion

4.1. Faithful representations of noise stimuli by FFR_{TFS} and FFR_{ENV}

In agreement with previous studies (e.g., Aiken and Picton, 2008; Ananthakrishnan et al., 2016; Skoe and Kraus, 2010; Wang and Li, 2015), the results of this study showed that both the FFR_{TFS} and FFR_{ENV} accurately conveyed the TFS and envelope information of the noise stimulus, respectively. Specifically, both the FFR_{TFS} and FFR_{ENV} showed markedly stronger coherence with the actually presented NBN relative to that with an irrelevant, uncorrelated NBN. Since the coherence analysis measures linear synchrony and requires both constant phase shift and amplitude ratio between the two signals to achieve a high coherence value (Levy et al., 2000; Middleton et al., 2006; Rosenberg et al., 1989), the neural representation of spectral features of NBNs by FFR_{TFS} and FFR_{ENV} described here can be considered as being largely relied on linear processing.

4.2. Sensitivity of FFR_{TFS} and FFR_{ENV} to ITD under the single-source condition

In this study, the FFR_{TFS} and FFR_{ENV} exhibited different sensitivity to ITD-cued perceived stimulus location. For the FFR_{TFS} , the ability to synchronize with the "target" sound was significantly dependent on the ITD, with the ipsilateral-leading sound eliciting markedly stronger S-R coherence than the contralateral-leading sound. Similarly, in previous reports, the amplitude of FFR_{TFS} to pain chatter (Du et al., 2009), harmonic complex (Ping et al., 2008), and pure tone bursts (Wilson and Krishnan, 2005) were ipsilaterally predominant. However, the IC FFR_{ENV} remained largely unchanged across different ITD conditions.

The lack of ITD tuning in FFR_{ENV} seems to be contrary to previous psychophysical studies showing that human listeners are sensitive

to the envelopes of high-frequency carriers (Henning, 1974; McFadden and Pasanen, 1976) and the fact that envelope-ITDsensitive neurons have been found in animal IC (e.g. Batra et al., 1989; Batra et al., 1993; Griffin et al., 2005; Smith et al., 2008). However, behavioral studies have also revealed that this sensitivity is not only highly listener-dependent (Macpherson and Middlebrooks, 2002: Trahiotis and Bernstein, 1986), but also typically weaker comparing with the sensitivity to the ITD cues in lowfrequency stimuli (Bernstein and Trahiotis, 1982; Wightman and Kistler, 1992; Yost et al., 1971). For example, the lateralization of high-frequency NBN has been shown to be relied on ITD cues conveyed by the low-frequency component of the stimulus more than the envelope ITD of the high-frequency sound itself (Bernstein and Trahiotis, 1982). The relatively poorer ability to use envelope ITD cues observed in psychophysical studies is supported by some neurophysiological studies showing that in IC neurons the tuning to envelope ITDs is much less sharp comparing with that to TFS ITDs (Griffin et al., 2005; Smith et al., 2008). One exception has been reported for the so-called "transposed tones", with which IC neurons showing an envelope-ITD sensitivity that is comparable to the TFS-ITD sensitivity (Griffin et al., 2005). This type of sounds has a distinct "off period" in the envelope (i.e. sufficiently long intervals with minimum envelope amplitude in each period), which elicits phase-locking responses to the stimulus envelope better than the traditional amplitude-modulated tones (Griffin et al., 2005). Moreover, a model simulation suggests that the intrinsic envelope of high-frequency Gaussian noise is not salient enough to convey ITD information (Macpherson and Middlebrooks, 2002). According to these previously reported findings, the envelope ITD cues in the NBN sounds may be too weak for the IC neurons to be detected. Thus, the results of this study suggest that TFS signals and envelope signals of NBN sounds, along with the embedded ITD cues, are processed separately in the IC. It is worth mentioning that the stimulus-response-coherence metric used in this study can only reflect the neural coding based on linear mapping of stimulus spectral features (Middleton et al., 2006). Non-linear processing of envelope ITD cues may also be involved, but cannot be revealed by the stimulus-response-coherence analysis. It is of interest to compare the envelope sensitivity of higher-order auditory centers with that of the IC.

The differences between FFR_{TFS} and FFR_{ENV} in sensitivity to ITD also suggest possibly different neural origins of these two FFR components. Previous studies (Ruggles et al., 2012; Shinn-Cunningham et al., 2013) have suggested that the tonotopic peripheral channels may have different contributions to FFRs: the FFR_{TFS} is mainly driven by frequency channels that are tuned to the stimulus frequency, while the FFR_{ENV} is mainly driven by mid- to high-frequency channels. This hypothesis is further supported by the findings that the phase-locking strength of scalp-recorded FFR_{TES} and FFR_{ENV} in humans are not correlated with each other (Ruggles et al., 2012), in agreement with our results showing a lack of correlation between the S-R coherence of FFR_{TFS} and that of FFR_{ENV}. Evidences from computational models and neurophysiological recordings (Carney et al., 2015; Wang and Li, in press) have suggested the involvement of IC neurons with different temporal processing properties in the representation of acoustic signals. More specifically, Carney's model shows that neurons with bandreject or low-pass modulation transfer functions (MTFs) tune to quickly fluctuated vowel formants, while neurons with bandpass MTFs tune to slowly fluctuated amplitude modulation (Carney et al., 2015). A recent FFR model based on this hypothesis has successfully separated FFR_{TFS} and FFR_{ENV}, and the simulated neural activity can well predict the FFR_{TFS} and FFR_{ENV} to NBN sounds recorded in rat IC (Wang and Li, in press). It is of importance for future studies to examine the roles of different types of IC neurons in the formation of FFRs and binaural processing.

4.3. Binaural release from masking for FFR_{TFS}

The results of this study provide evidence showing that, when perceived spatial separation is established through the introduction of ITD disparity between the concurrent sounds, the FFR_{TFS} benefits from the spatial cues and displays better synchronization selectively to the sound that is perceived from the ipsilateral ear.

TFS information has been shown to play an important role in speech perception (Hopkins and Moore, 2010; Lorenzi et al., 2006), especially when target speech is presented with temporally fluctuating background noises (Gnansia et al., 2008; Hopkins and Moore, 2009; Hopkins et al., 2008; for a review, see Moore, 2008). In a recent study examining the human scalp-recorded FFRs to noise-degraded speech, stronger response-stimulus correlation was found for the TFS component than that for the envelope component (Bidelman, 2016). Deficit in excessing TFS cues due to excessive encoding of envelope information has also been proposed to cause difficulties in understanding target sounds in noise for listeners with hearing loss (Anderson et al., 2013; Kale and Heinz, 2010). The better representation of individual sounds by FFR_{TES} when sounds are spatially separated may lead to improved perceptual performance, and hence serve as a "bottom-up" neural basis for the behavioral phenomenon general known as "spatial release from masking" (SRM).

Consistent with our findings, previous studies in both rats (Du et al., 2009) and humans (Wilson and Krishnan, 2005) have reported that FFRs can be unmasked by binaural spatial cues. Further, Lane and Delgutte (2005) have also reported the SRM effect in the population neural responses of cat IC. However, there is one fundamental difference in stimulus choosing when comparing these studies to ours: the maskers used in these previous studies are all broadband noises, hence lack the pronounced periodicity possessed by the target signals, which turned out to be able to significantly influence the neural responses (Lane and Delgutte, 2005). In this study, the two concurrent sounds were both NBNs with the same spectrum range, therefore the cues introduced by physical differences were strictly limited, making it very difficult to resolve individual sounds. Nevertheless, the results of this study indicate that IC neurons can achieve the segregation of sounds with the identical spectra based on ITD disparity.

Keller and Takahashi (2005) have shown that when two amplitude-modulated broadband noises with completely overlapping spectra were presented spatially separated at the same time, the neurons in the external nucleus of IC of barn owls could separate the concurrent sounds using binaural cues even when the two sounds shared the identical envelope. Therefore, they proposed that source separation at the level of midbrain is mostly based on TFS information. However, whether and how the detailed TFS information is preserved is not clear. From this perspective, we have extended the previous understanding of sound segregation at the brainstem level, and demonstrated that the TFS component of FFRs precisely conveys TFS information of acoustic signals with a relatively high signal-to-noise ratio when concurrent sounds are in perceived spatial separation conditions. Thus, FFRs are useful for investigating the neural representation of complex auditory scenes including the presentation of concurrent sounds with overlapping spectra.

4.4. Concurrent sound segregation is reflected by FFR_{TFS} and FFR_{ENV}

The results of this study indicate that FFR_{TFS} , but not FFR_{ENV} , reflects the unmasking effect of ITD cues for concurrent sounds. Therefore, our study for the first time provides evidence suggesting

that FFR_{TFS} and FFR_{ENV} reflect differentially the coding of concurrent sounds in the rat IC. To our knowledge, only few reports have investigated the differences between TFS and envelope in sound segregation based on spatial localization. As mentioned above, Keller and Takahashi (2005) have shown that source segregation of spatially separated sounds at the level of midbrain is relied on differences in TFS while no evidence on envelope-based grouping is observed. Meanwhile, in a behavioral study employing a speech identification task with competing speech maskers, Swaminathan et al. (2016) have shown that the absence of TFS information in low-frequency channels (below 1500 Hz) results in a decreased beneficial effect of SRM, even though the spatial cues in envelope are fully preserved. These findings, along with those of this study, suggest a critical role of TFS in the segregation of concurrent sounds when spatial processing are involved; meanwhile the envelope cues may be less useful in the segregation. A computational model simulating the peripheral auditory system has demonstrated that, comparing with envelope cues, TFS cues are more robust in noisy environment in the early stage of auditory processing, represented by the less degraded phase-locking to the stimulus TFS in the auditory nerve (Shamma and Lorenzi, 2013). Thus, central auditory system may give more weight to the noise-resistant TFS cues in the processing of concurrent sounds.

On the other hand, considering the importance of envelope cues to speech intelligibility both in quiet (Shannon et al., 1995; Smith et al., 2002) and in noise (Swaminathan and Heinz, 2012), perceiving target-speech signals with concurrent masker presentation may require that envelope information of individual sounds is successfully resolved. Although in this study, no signs of interactions between TFS and envelope processing was found at the level of brainstem, it is of great interest to ask whether and how higher auditory centers can use the TFS-based sound segregation processing to facilitate the retrieval of intelligibility information conveyed by envelope. Ding et al. (2014) have provided imaging evidence showing that the cortical entrainment to speech envelope is not a simple representation of envelope, but a collective representation of auditory features that rely on the intactness of TFS information, indicating an integration of TFS and envelope information at the cortical level. Further studies are needed to investigate how the processing of TFS and that of envelope are integrated and the associated auditory pathway.

5. Conclusions

When two or more sounds with overlapping spectra are presented at the same time, spatial information serves as an important cue for auditory segregation. This study used uncorrelated NBN pairs to simulate this scenario and revealed both the TFS and envelope components of the phase-lock-based FFRs that were elicited in the rat auditory midbrain IC. The FFR_{TFS}, but not the FFR_{ENV}, shows the sensitivity to ITD and better synchronizes with the sound that is perceived from a preferred location when perceived spatial separation between the concurrent sounds is established due to the ITD disparity.

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